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(54) Intraluminal stent for attaching a graft

Intravaskulärer Stent zur Befestigung einer Prothese

Stent endoluminal pour fixer une prothèse vasculaire

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EP-A- 0 497 620	EP-A- 0 539 237
EP-A- 0 540 290	EP-A- 0 551 179
EP-A- 0 621 016	EP-A- 0 657 147
EP-A- 0 686 379	WO-A-92/06734
DE-A- 4 303 181	US-A- 3 657 744
US-A- 5 064 435	US-A- 5 104 399
US-A- 5 397 355	

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Description**BACKGROUND OF THE INVENTION**

[0001] The invention relates generally to endoprostheses and, more specifically, to intraluminal grafts and devices for delivering and deploying the same to an area of a body lumen that has been weakened by damage or disease, such as by an aneurysm of the abdominal aorta.

[0002] An abdominal aortic aneurysm ("AAA") is an abnormal dilation of the arterial wall of the aorta in the region of the aorta that passes through the abdominal cavity. The condition most commonly results from atherosclerotic disease. Frequently, abdominal aortic aneurysms are dissecting aneurysms, that is aneurysms that are formed when there is a tear or fissure in the arterial lining or wall through which blood is forced and eventually clots, forming a thrombosis which swells and weakens the vessel. Abdominal aortic aneurysms do not cause pain, but are easily detected in a thorough physical examination. If the aneurysm is not detected and treated, it is likely to rupture and cause massive hemorrhaging fatal to the patient.

[0003] Treatment of AAAs comprises some form of arterial reconstructive surgery which commonly is referred to as a "triple-A" procedure. One such method is bypass surgery, in which an incision is made into the abdominal cavity, the aorta is closed off above and below the site of the aneurysm, the aneurysm is resected, and a synthetic graft or tube sized to approximate the diameter of the normal aorta is sutured to the vessel to replace the aneurysm and to allow blood flow through the aorta to be re-established. The graft commonly is fabricated of a biocompatible material that is compliant and thin-walled. Nylons and synthetic fibers such as those manufactured under the trademarks DACRON or TEFLON have been found to be suitable for the construction of the graft. Studies have shown that the mortality rate associated with this surgical procedure is favorable (less than 5%), when it is performed prior to rupture of an aneurysm. However, patients having an AAA typically are over 65 years of age, and often have other chronic illnesses which increase the risk of perioperative or post-operative complications. Those patients thus are not ideal candidates for this type of major surgery. Further, it has been pointed out that this procedure is not often successful after an aneurysm has ruptured (the mortality rate increases to over 65%), because of the extensiveness of the surgery and the time required to prepare a patient for the procedure.

[0004] Because of the aforementioned disadvantages to conventional surgical methods, another procedure was developed as an alternative to conventional, major surgery. This method also involves emplacement of a graft at the site of the aneurysm; however, the graft is deployed there by being carried by a catheter, wire or other device suitable for negotiating the vasculature

which is routed through the vascular system to the target area for treatment. The graft and its deployment system often are introduced into the blood stream percutaneously with a femoral approach and the entire procedure can be performed using local rather than general anesthesia.

[0005] Once the graft has been positioned at the aneurysm, it is disengaged from the delivery system and can be affixed to the aortic wall both distally and proximally of the aneurysm. For this purpose, grafting systems usually include fixation means such as staples or hooks which can be manipulated and driven into the intima of the vessel via some mechanical feature of the system or, alternatively, by some physical process, such as by expansion of the graft through the application of pressure or a temperature change. To avoid premature detachment of the graft and to prevent the attachment elements from damaging the vessels or halting the forward movement of the system while the graft is being routed to the treatment site, the systems often are provided with a feature such as a capsule or a sheath that protects and contains the graft until such time as deployment is desired.

[0006] Once the graft is in place, it is positioned in the vessel spanning the site of the aneurysm such that the walls of the graft are generally parallel to the walls of the affected area of the aorta. The aneurysm thus is excluded from the circulatory system by the graft rather than being resected altogether. If the aneurysm is a dissecting type and a thrombosis exists between the walls of the aorta, the now-excluded aneurysm may beneficially provide structural support for the graft.

[0007] Grafting systems are known that include what commonly is referred to as an attachment system for deploying the graft. The attachment system is a tubular device which is fitted inside and is generally coaxial with the graft, and which can extend out of the graft at either or both the proximal and distal ends thereof. The attachment system often has a lattice-like or open-weave structure, that provides it with flexibility and which promotes rapid endothelial tissue growth through the structure once the graft has been deployed. It may be provided with additional hook-like elements for penetration of the intimal walls for attachment of the graft to the aorta, or such hook-like elements may be provided on the graft itself. Graft systems of type described can be found in U.S. Patent Nos. 4,787,899 (Lazarus); 5,104,399 (Lazarus).

[0008] The actual function of delivering the graft may be accomplished by inflating a balloon of a catheter, by introducing pressurized fluid into a lumen of the catheter from a source external to the patient. Inflation of the balloon applies a force to the graft and any attachment system supplied therein. This force extends radially and presses the graft and attachment system into the vessel wall just above and just below the aneurysm. When an attachment system is used, disengagement of the catheter from the graft also has been accomplished by taking

advantage of the chemical properties of the material from which the attachment system is manufactured. For example, a prior art attachment system is known that is in the form of a coil of an nickel-titanium alloy, manufactured under the trademark NITINOL™, that will expand radially upon being heated to a higher temperature. The longitudinal dimensions of any attachment system used must account for any reduction in length that might result from radial expansion of the device. Other devices used to attach a graft to the aortic wall for AAA repair include intravascular stents of the type found in U.S. Patent No. 4,733,665. Other forms of stent are described in WO-A-9,206,734 and EP-A-0,540,290 while other forms of aortic graft are described in EP-A-0,551,179 and EP-A-0,539,237.

[0009] WO-A-9,206,734 describes a self-expanding endovascular stent that holds a passageway enlarged by placing the stent into a lumen. The stent comprises a cylindrical frame formed by a plurality of unit structures each formed into a closed zig-zag configuration including an endless series of straight sections and joined by bends. Connecting members are provided which connect the unit structures while a mesh is wrapped around an outside of the frame.

[0010] Likewise, EP-A-0,540,290 describes an expandable stent for implantation in a body lumen, such as an artery. The stent consists of a plurality of radially expandable cylindrical elements generally aligned on a common axis and interconnected by one or more interconnective elements. The individual radially expandable cylindrical elements consist of ribbon-like material disposed in an undulating pattern.

[0011] By contrast, EP-A-0,551,179 describes a bilateral intra-aortic bypass graft and a method and apparatus for repairing an abdominal aortic aneurysm including two tubular grafts which are intraluminally delivered to the aorta and secured to the aorta by the expansion and deformation of two expandable and deformable tubular members.

[0012] EP-A-0,539,237 describes a transluminal grafting system for grafting a prosthesis to the wall of a lumen comprising a tubular graft provided with spring assemblies and anchoring barbs. The prosthesis is mounted on an apertured tubular carrier and a central control means is inserted into the bore of the apertured carrier. Mooring loops are attached to the prosthesis, pass through the apertures of the tubular carrier, and engage the central control means. An introducer sheath covers the system for smooth insertion into a lumen. When the graft has been positioned, the central control means maintains the axial position of the prosthesis. When the introducer sheath is pulled, the prosthesis is exposed and the spring assemblies return to an expanded state and anchor the graft against the internal wall of the lumen.

[0013] In order for a stent to be used most advantageously with a graft deployment system for treatment and repair of aneurysms, the stent must be composed

of a biocompatible material. The stent simultaneously must be flexible enough to comply with the catheter or other element used to route the graft through the often tortuous vascular path to the site of the aneurysm and strong enough radially to maintain the opening in the graft once delivered. The stent must be well suited to deployment by a delivery system that is not overly complex, and thus is reliable and easy to operate. Further, it is desirable that the stent be expandable, so that upon application of a force or physical change from within, which is sufficient to cause its radial expansion, the stent encourages affixation of itself and of the graft to the aortic walls. Although various graft delivery systems have been proposed, none adequately provides all of these desirable features.

[0014] What has been needed and heretofore unavailable is a stent for use in combination with a graft which has a high degree of flexibility for efficient advancement through tortuous passageways, which can be radially expanded from a relatively small diameter to a relatively large diameter without substantial longitudinal contraction, and which exhibits mechanical strength sufficient to adhere to the vessel walls and to maintain the patency of a synthetic graft implanted at the site of an aneurysm.

SUMMARY OF THE INVENTION

[0015] According to a first aspect of the present invention there is provided an intravascular stent for implanting in a body lumen, comprising: a plurality of cylindrical elements which are independently expandable in the radial direction and which are interconnected so as to be generally aligned on a common longitudinal axis, each cylindrical element having a serpentine pattern of alternating peaks and valleys; a plurality of connecting elements for interconnecting said cylindrical elements, said connecting elements configured to interconnect only said cylindrical elements that are adjacent to each other so that said stent, when expanded in the radial direction, retains its overall length without appreciable shortening; and said stent being characterised in that it further comprises a plurality of hooks for attaching said stent to the body lumen, each hook being provided at a respective peak of a cylindrical element at a first end of said stent, said hooks extend from said first end of said stent in a direction away from said stent and generally parallel to said common longitudinal axis.

[0016] Particular embodiments of the invention are directed to a stent for use with catheter-graft delivery systems for repairing diseased or injured vessels, and most notably for treating aneurysms, especially aneurysms of the abdominal aorta. The stent is expandable, so that a low profile can be maintained while the graft-and-stent combination is being routed to the aneurysm, and then expanded at the time of deployment to a diameter roughly approximating the diameter of a healthy abdominal aorta and the final diameter of the tubular-shaped

graft. Tubular grafts used in the delivery system are conventional and are well known in the art. However, the stent that is disposed within the graft is novel and unique. It has a configuration that allows it to expand radially to a much larger diameter than was heretofore possible, and is provided with hooks to penetrate the aortic wall at least above the aneurysm to anchor the graft. The stents are somewhat flexible along their longitudinal axis to facilitate delivery to the treatment site through tortuous blood vessels, but in the expanded condition they are radially stable enough to maintain the patency of the graft and aorta and to attach the combined structure to the aortic walls.

[0017] Thus, according to a second aspect of the present invention there is provided a graft-and-stent assembly for repairing an aortic aneurysm, the assembly comprising: an expandable tubular graft having a distal end and a proximal end and having a length sufficient to span the aortic aneurysm so that said distal end and said proximal end may be positioned adjacent healthy aortic tissue; an expandable stent affixed to said graft, said stent extending for at least a length distally of said graft such that upon expansion of the graft-and-stent combination at least a first portion of said stent will extend distally of said distal end of said graft; said stent having a plurality of cylindrical elements which are independently expandable in the radial direction and which are interconnected so as to be generally aligned on a common longitudinal axis, each cylindrical element having a serpentine pattern of alternating peaks and valleys; a plurality of connecting elements for interconnecting said cylindrical elements, said connecting elements configured to interconnect only said cylindrical elements that are adjacent to each other so that said stent, when expanded in the radial direction, retains its overall length without appreciable shortening; said stent further including a plurality of hooks on said distally-extending portion of said stent for engaging the aortic wall distally of the aneurysm and affixing the graft-and-stent combination to repair the aortic aneurysm, each hook being provided at a respective peak of a cylindrical element at a most distal end of said stent, said hooks extending from said most distal end of said stent in a direction away from said stent and generally parallel to said common longitudinal axis; and catheter means for delivering and deploying said stent and said graft, said catheter means having a balloon portion for radially expanding said stent into engagement with the aortic wall.

[0018] As used herein, reference to the "proximal" is toward the exterior of the patient and away from the stent and graft, while reference to the "distal" is toward the stent and graft on the balloon portion of the catheter. The proximal and distal references apply to directions in the vascular system and especially to the aorta.

[0019] In a preferred embodiment, a stent is attached to the distal end of a tubular graft such that at least a portion of the stent is exposed distally beyond the distal end of the graft. The graft-and-stent are deployed intra-

luminally such that the stent and the distal end of the graft are positioned distally of the aneurysm while the proximal end of the graft extends proximally of the aneurysm. The distal end of the stent is provided with attachment hooks for penetrating healthy tissue in the aortic wall above the aneurysm in order to attach the graft-and-stent combination to the aortic wall. The attachment hooks can have multiple configurations as described herein. Due to the high pressures associated with blood

10 flow in the aorta, it may be unnecessary to provide attachment hooks in the proximal end of the graft since the graft will be held in place by the pressure of the blood flow. However, under certain conditions, attachment hooks in the proximal end of the graft may be desirable.

15 [0020] Thus, in one embodiment, a pair of stents are attached to a tubular graft, one stent at the proximal end and one stent at the distal end of the graft. The stents are oriented so that when both the graft and the stents are expanded to larger diameter states, the stents will 20 be coaxial with the graft. The portions of the stent extending out of the graft are affixed with hooks for penetrating healthy tissue in the walls of the aorta above and below the aneurysm, to aid in attaching the combined structure to the aortic wall. The hooks can have multiple 25 configurations such as one or more barbs, and the barbs can be of various shapes, containing one or more angles, so that the hooks effectively will anchor the graft-and-stent combination to the aortic wall.

[0021] The graft-and-stent combination is readily delivered to the aneurysm by mounting it on a balloon portion of a delivery catheter, and passing the catheter-graft-stent assembly through the vasculature to the implantation site. A variety of means for securing the graft-and-stent combination to the catheter during delivery is 30 available. Presently, it is preferred to compress the stent onto the balloon, and to retain the stent and the graft on the balloon using a protective sheath.

[0022] Other features and advantages of the present invention will become more apparent from the following 35 detailed description of the invention, when taken in conjunction with the accompanying exemplary drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

45 [0023] FIGURE 1 is a plan view depicting the stent having hooks at one end and prior to rolling it into a cylindrical configuration.

[0024] FIG. 2 is a perspective view of a portion of the 50 stent of FIG. 1 rolled into a cylindrical configuration with only the top ring fully depicted for clarity.

[0025] FIG. 3 is a perspective view of a portion of the stent of FIG. 1 rolled into a cylindrical configuration and expanded, again with only the top ring fully depicted for clarity.

55 [0026] FIG. 4 is a plan view depicting a stent in a flattened form and having support bars on the edges for welding when the stent is rolled into a cylindrical form and depicting spikes for attachment means.

[0027] FIG. 5 is a plan view of a stent depicting lap joints which mate when the stent is rolled into a cylindrical configuration.

[0028] FIG. 6 is a plan view of the stent depicting an alternate embodiment of the invention having attachment hooks with barbs.

[0029] FIG. 7 is an enlarged partial plan view of the stent of FIG. 6 depicting the attachment hooks having barbs.

[0030] FIG. 8 is an elevational view, partially in section, of the stents incorporated into a graft and of a delivery system, which can deliver and deploy the stents and graft.

[0031] FIG. 9 is an enlarged partial view of one of the stents shown in FIG. 8 attached to the graft.

[0032] FIG. 10 is an elevational view, partially in section, of the stent, graft, and delivery system of FIG. 8, after the graft-and-stent combination has been advanced and deployed in the region of an aneurysm and the stents have been deployed.

[0033] FIG. 11 is an elevational view, partially in section, of the graft-and-stent combination of FIGS. 9 and 10, after the combination has been deployed and the catheter withdrawn.

[0034] FIG. 12 is an elevational view, partially in section, of another means by which a stent embodying the invention can be incorporated into a graft delivery system, depicting the system prior to advancement of the graft-and-stent combination into the region of an aneurysm.

[0035] FIG. 13 is an elevational view, partially in section, of the delivery system of FIG. 12 after the graft-and-stent combination has been advanced and partially deployed in the region of an aneurysm.

[0036] FIG. 14 is an elevational view, partially in section, of an alternate means by which a stent embodying the invention can be incorporated into a graft delivery system, depicting the system prior to deployment of the graft-and-stent combination.

[0037] FIG. 15 is an elevational view, partially in section, of the delivery system of FIG. 14, depicting the system during deployment of the graft-and-stent combination.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0038] The invention relates to an intravascular stent, one or more of which is used in conjunction with a known tubular graft for repairing body lumens of all types. As described herein, reference is made to repairing an aortic aneurysm, however, other body lumens are equally suited to receive the graft-and-stent combination of the present invention.

[0039] FIG. 1 depicts a stent 10 embodying features of the invention, in the state the stent would appear if flattened prior to rolling into a cylindrical configuration. The stent generally is comprised of a plurality of cylind-

rical rings 12 which are spaced close enough together to allow the stent to provide a reliable means of attaching the graft at the treatment site, but are not so tightly spaced as to inhibit the flexibility of the combination. The

5 cylindrical rings are connected to each other by connecting members 14. Each cylindrical ring is characterized by a serpentine or wave pattern, having a series of alternating peaks 16 and valleys 18. The degrees of curvature indicated by arrows B along adjacent peaks and
10 valleys are different and, preferably, the pattern of each cylindrical ring is in phase with the pattern of every other cylindrical ring. Attachment elements 20, shown in FIG. 1 in the form of hooks, are provided on a first end 22 of the stent, to engage with the aortic wall when the stent
15 is deployed. A second end 24 of the stent will be attached to the graft when the graft-and-stent combination is assembled. As is described more fully below in relation to FIGS. 8-11, when two stents 10 are used in combination with a single graft, only the stent situated at the
20 most distal end of the graft need be provided with attachment elements in order to adequately anchor the combination to the vessel. In FIG. 1, the configuration of the hooks is such that each is positioned at every other peak 18 that is at the first end 22 of the stent, which
25 will comprise the most distal end of the stent when it is fully formed and oriented for deployment. Each hook has a shaft portion 32 extending outwardly from the distal most cylindrical ring, and a barb portion 34 extending from the shaft.

30 [0040] The expansion properties of stainless steel make it a preferred material for the stent 10. As is set forth more fully below, the stent, including the hooks, can be formed from a flat sheet of material by chemically etching, laser cutting, or electronic discharge machining (EDM) and the like. It also is contemplated that the hooks may be formed independently of the stent and subsequently attached to it by welding, brazing or another process with the equivalent effect. The body has width W and length L, which length will be parallel with
35 a longitudinal axis A of the stent when the body is rolled into a cylinder. To secure the cylinder, lengthwise edges 28 and 30 of the body can be connected with a suitable means such as by welding, brazing, soldering or with adhesives. A yttrium-YAG laser is particularly suitable
40 for welding the lengthwise edges 28,30 together (See FIG 2).

45 [0041] In a presently preferred embodiment, as shown in FIG. 1, it is contemplated that a stent with the dimensional characteristics disclosed below would be suited for use with a graft in triple-A procedures with a variety of vascular anatomies. It is clear, however, that a stent with other dimensions might be equally useful in a graft delivery procedure. Preferably, the stent 10 is formed from a flat sheet of stainless steel. For a flat sheet, prior to being rolled into a cylindrical shape, width W of the stent is approximately 16 millimeters (0.63 inches), while length L of the stent exclusive of hooks 20, is in the range of about 5.1 to 50.8 millimeters (0.2 to 2.0

inches). It is desirable for the connecting members 14 to have a transverse cross-section similar to the transverse dimensions of the undulating components of the expandable bands. The shaft of each hook has length C of approximately 1.3 millimeters (0.05 inch) and diameter (or width) D of approximately 0.2 millimeters (0.008 inch). The barbs of the hooks have width E of approximately 0.8 millimeters (.03 inch). As stated, these dimensions are preferred, but the selection of the most appropriate dimensions in a particular clinical situation may vary considerably from patient to patient.

[0042] After the stent 10 has been rolled into its cylindrical shape from a flat sheet, as seen in FIG. 2, the features of the device are such as to allow the stent to be uniformly expanded in a radial direction, FIG. 3, both to a significant degree and without large variation in the level of diametric expansion of each cylindrical ring. The cylindrical rings 12 are transverse to the longitudinal axis A of the finished stent, and the varying degrees of curvature B between peaks 16 and valleys 18 tend to equalize the stresses experienced by the stent during expansion, so that the peaks and valleys of each band deform radially with substantial uniformity upon application of an expansion force. The structure permits the stent to increase from an initial, small diameter to any number of larger diameters (See FIG. 3). When the interconnections 14 between two cylindrical rings are aligned with the interconnections between all other cylindrical rings, such that the attachment is accomplished by traversing the distance between the peaks 16 of consecutive cylindrical rings, the serpentine pattern of each cylindrical ring is in phase with the pattern of every other ring. This manner of connection of the cylindrical rings thus minimizes the degree to which the stent will be shortened or will contract along its longitudinal axis A. This configuration also limits twisting of the stent upon expansion and it enhances more uniform expansion. The in-phase cylindrical ring patterns further are thought to reduce the likelihood that the stent or any portion of it will recoil, or collapse back to its starting diameter after deployment.

[0043] The number and orientation of the connecting members of the stent 10 can be varied in order to maximize the desired longitudinal flexibility of the stent structure both in the unexpanded and in the expanded condition. Flexibility is advantageous during deployment of the graft and stent because it improves the ease and safety with which the combination can be delivered through the vascular system to the aneurysm. Following affixation of the stent to the aortic wall, longitudinal flexibility minimizes alteration of the natural physiology of the aorta due to the implant and helps to maintain compliance of the portions of the vessel supporting the graft. The discrete bands also have the capacity to rotate slightly with respect to each other without causing any significant alteration of the basic cylindrical structure of the stent. Accordingly, the cylindrical rings and connec-

tions cumulatively result in a stent that is very flexible along its length or longitudinal axis, but which provides uniform expansion and is very stable and resistant of collapse. The reticulated structure supplied by the patterning allows for the perfusion of arterial blood into the region of the aortic wall to which elements 14 are attached to anchor the graft and stents or graft and stent in place. Such perfusion promotes assimilation of the synthetic prostheses by the aorta and, more generally, healing of the treated site.

[0044] The more uniform radial expansion of this design results in a stent 10 that can be expanded to a large diameter without substantial out-of-plane twisting, because no high stresses are concentrated in any one particular region of the serpentine or wave pattern. Rather, the forces are evenly distributed among the peaks 16 and the valleys 18, allowing the cylindrical rings 12 to expand uniformly. Minimizing the cut-of-plane twisting experienced by the stent during delivery and deployment of the graft-and-stent combination also carries with it the benefit of minimizing the risk of thrombus formation. The special expansion characteristics of the stent of the invention also allow any portion of the stent that extends distally or proximally of the graft to continue to expand even when the graft has achieved its maximum cross-sectional dimension, so as to more securely affix the graft-and-stent combination to the vessel above and below the aneurysm.

[0045] The uniformity in stress distribution further reduces the likelihood that fractures in the stent 10 will occur due to stresses applied to any particular region or cylindrical ring 12 of the stent. This feature also contributes to the ability of the stent to be expanded to a greater degree and at a faster rate than was feasible previously with other designs. Radial strength is not sacrificed upon expansion and the degree to which expansion causes longitudinal contraction, and thus a shortening of the stent, is minimal.

[0046] In FIG. 4, the attachment elements 20 are in the form of spikes rather than hooks, being straight and having sharply pointed tips at the end of the shafts. The length C and the length F of shafts 32 and tips 40 respectively, are approximately 1.3 millimeters (0.05 inch). When the stent 10 is expanded, some of peaks 16 or valleys 18 of the cylindrical ring 12, or portions thereof, which extend distally or proximally of the graft, may tip outwardly, becoming embedded in the aortic wall and forcing the spikes also to become lodged in the vessel, thus aiding in retaining the stent in place as the stent becomes permanently implanted. Support bars 36 are provided at lengthwise edges 28 and 30 of the stent body 26, to provide support material for a joint. As the stent 10 is rolled into a cylindrical form, the edges 28,30 can abut or overlap and then can be permanently affixed to each other by known means such as laser welding, brazing, soldering, epoxy, and the like.

[0047] Still another design of stent is shown in FIG. 5. As in FIG. 4, the attachment elements 20 are configured

as spikes instead of as barbed hooks. In lieu of support bars 36, the lengthwise edges 28 and 30 of stent body 26 are provided with lap joints 38, which allow the stent to be mechanically secured as a cylinder. The lap joints 38 are configured to mate when the stent 10 is rolled into its cylindrical configuration. The lap joints 38 are attached to each other by welding, brazing, soldering, or the application of an epoxy or an adhesive. Attachment hooks 20 having a barb portion 34 also may be formed on the stent end opposite attachment spikes shown in FIG. 5.

[0048] Another embodiment of the attachment elements 20 is illustrated in FIGS. 6 and 7. Barbs 34 with dimensions similar to those of the barbs of FIG. 1 are provided, however, the barbs further are equipped with tail portions 42, which have length G of approximately 1.3 millimeters (0.05 inch). Again, the dimensions set forth herein only are for illustration purposes and will vary widely depending upon the application and the patient. It readily can be appreciated that many other types of hook may be affixed to or formed unilaterally with the stent body without departing from the scope of the invention. For example, multiple barbs can be provided spaced apart from each other on the shaft of a single attachment element for more than one anchor site per element. The angles formed between the shafts and barbs can vary and can be selected so as to best accomplish the anchoring function in a given application. Many other shapes and configurations are contemplated that are designed to optimize the attachment of the end of the stent to the aortic wall while the healing process is taking place to assimilate the stent and graft into the vessel by endothelial tissue growth.

[0049] Details of the various processes by which the stainless steel stent can be manufactured can be found in co-pending EP-A-662 307 and US-A-5 421 955. Briefly, the stainless steel stent can be formed by a chemical etch process out of a flat sheet or a piece of tubing. The areas of stainless steel to remain are identified by covering the regions with a material resistant to the chemicals used in the etching process, such that when the metal is exposed to the chemicals, the openings or reticules in the patterned structure are created by reaction of the chemicals with the unprotected areas of the steel. The etching process develops smooth openings in the sheeting or tubing devoid of burrs or other artifacts that can be characteristic of other processes when products of the small sizes contemplated here are manufactured. An electropolishing process may be used after the chemical etching is complete in order to polish the stent surface. The stent surface can be polished to an approximately 12.7 to 25.4 micron (5 to 10 micro inch) finish.

[0050] There are numerous advantages in chemically etching a flat sheet of material, such as a stainless steel, into a stent embodying the invention. For example, chemical etching is economical since a large number of stents can be chemically etched on the same flat sheet at the same time. The chemical etching process creates

no burrs and the surface finish of the eventual inside diameter of the stent can be improved by electro-polishing on one side only. Further, chemical etching creates no extra heat treating to the parts that are being processed. The raw material wall thickness and grain structure is more uniform in a flat sheet as opposed to chemical etching a stainless steel tube. Further, in a flat sheet, the bevel of the etching can be controlled, whereas when tubing is etched, the bevel creates a thicker part 10 on the inside diameter and a thinner part on the outside diameter.

[0051] An important advantage of chemical etching the stent from a flat sheet of stainless steel material is that a process known as "step etching" can be used. For example, by using step etching in the areas of the spikes 20 in FIG. 4, it is possible to remove portions of material so that the spikes will bend outwardly when the stent is expanded. In other words, step etching allows for the removal of material in highly selective areas so that upon radial expansion of the stent, areas having less material will have a tendency to bend or distort, such as with the spikes bending outwardly to engage the aortic wall.

[0052] Photo-lithographic techniques also can be employed for the manufacture of the stents, using a computer-controlled laser patterning process to remove the chemically resistive coating applied to the metal sheet or tube. A plurality of stents can be formed from one length of sheeting or tubing, by repeating the stent pattern and providing small webs or tabs to interconnect the stents. After the etching process, the stents can be separated by severing the small webs or tabs. Subsequently, if the stents were formed on a sheet, the individual stents are rolled and the edges welded together 35 to provide a cylindrical configuration.

[0053] Yet another method of making a stent embodying the invention is by the commonly known process of electronic discharge machining (EDM). Using EDM, the stainless steel stent can be formed from a flat sheet or 40 from a section of tubing.

[0054] When the stent 10 is made from a material that is difficult or impossible to detect under fluoroscopy, such as stainless steel, it is desirable to incorporate radiopaque markers to identify the position of the graft-and-stent assembly during deployment. The stent 10 can be coated with a metal film that is radiopaque, such as gold, silver, platinum, tantalum and the like. One method of coating the stent with a radiopaque marker is disclosed in patent application EP-A-679 372.

[0055] One preferred method of incorporating the stent into a graft delivery system is illustrated in FIGS. 8-11. The delivery system 50 is used to deploy tubular graft 52 at the site of abdominal aortic aneurysm 54 via stents 56 and 58. The structure of stents 56 and 58, the materials from which the stents are made, and the processes that might be used to form the stents are set forth in detail in connection with the discussion of FIGS. 1-7. It is contemplated that this use of the stent could be ac-

complished with a wide variety of graft types. Due principally to the ability of the stent to expand rapidly from a very small diameter to a much larger diameter without substantial shortening, a stent with a relatively short length can be used. The graft used in this delivery system is sized so that its cross-section substantially matches that of the healthy portion of the aorta.

[0056] Delivery system 50 includes multilumen catheter 60 of the type used in other percutaneous procedures for deploying stents and other prostheses to repair portions of blood vessels. The catheter has a first lumen extending along its length which is in communication with two expandable members or balloons disposed at the distal end of the catheter. The balloons are spaced apart for a distance that is slightly less than the length of the shortest graft intended to be deployed using the system. Pressurized fluid or gas can be introduced into the balloon lumen to inflate the balloons, to exert an outward radial force on anything disposed about the balloon.

[0057] After the stents 56 and 58 have been attached to the graft 52, the graft-and-stent combination is loaded onto the distal end of catheter 60. The combination is positioned so that each stent overlies a balloon 62 and the graft rests over and is substantially coaxial with the portion of the catheter that is between the two balloons. In order to insure that the graft and stents remain in this position until the deployment function is accomplished, the two stents are compressed or "crimped" onto the balloons prior to insertion of delivery system 50 into the patient. The graft and stents also can be secured by positioning the stents between ridges or collars provided on the expandable members, which will restrain lateral movement of the combination. Alternatively, biodegradable adhesives might be used to temporarily affix the stents to the balloons, the adhesives being subject to degradation and absorption by the body when it is desired to deploy the graft.

[0058] The catheter 60 further is provided with a sheath 64 that helps to hold the graft and stents onto the catheter and which prevents direct contact of the elements of the combination with the walls of the vessels while the system is being advanced to the treatment site, thus protecting the vascular system of the patient from any sharp edges on the stents. A rod or wire 66 or other suitable mechanical element is connected to the sheath and extends proximally along the length of the catheter so that it can be manipulated by the physician exterior to the patient and retracted (proximally) at the time of deployment. Alternatively, a sheath can be provided that traverses the entire length of the catheter, and can be retracted (proximally) from outside the patient to expose the graft-and-stent combination.

[0059] The catheter has a second lumen through which guidewire 68 passes. The guidewire advantageously is advanced through the vasculature of a patient beyond the site of aneurysm 54 as a preliminary step in the graft delivery procedure. After the guidewire has

been positioned, the catheter carrying the graft and stents is advanced over the guidewire. Although a particular form of catheter has been described to route the graft-and-stent combination to the aneurysm, it will be apparent to those skilled in the art of treating aneurysms and similar conditions and of percutaneous catheter design that catheters of various configurations or wires and rods or the like could be used successfully to perform the same function. For example, well known fixed wire and rapid exchange wire systems also can be used in the delivery system described herein.

[0060] Attachment elements in the form of hooks 20 are provided on the most distal end 22 of the stent 58, which hooks ultimately will attach the graft-and-stent combination to regions in the intima or aortic wall. If desired or necessary to achieve a more secure attachment, hooks also can be provided on the proximal end of the stent 56 for attaching to the aortic wall 72 at a point proximal to the aneurysm. The hooks anchor the stents and the graft while the implantation process is ongoing, and before the body has naturally assimilated the combination through intergrowth of endothelial cells.

[0061] As is shown in FIG. 8, the stent 56 and the stent 58 each are affixed to an end of the graft 52 by staples 53. Other appropriate means might be used, such as a biocompatible adhesive, for example an epoxy resin, to attach the stents 56, 58 to the graft 52. Alternatively, the stent might be sewn onto the graft at selected points. At least a portion of the stents 56, 58 extend out of the graft 52, and if the stents and graft are joined by a butt joint, then substantially all of the stent will extend out of the graft.

[0062] In FIG. 8, all of the elements of the graft delivery system 50 except the distal end of the guidewire 68 are shown positioned proximally of the aneurysm 54, before the graft 52 and the stents 56 and 58 have been deployed. The sheath 64 of the catheter 60 covers the graft and stents disposed about the balloons 62, and the distal end of the guidewire has entered the region of the aorta that is affected by the aneurysm. In FIG. 10, the sheath is withdrawn (proximally) exposing the graft-and-stent combination and the catheter is advanced so that the graft-and-stent combination span the aneurysm. The balloons 62 are inflated by the pressurized fluid or gas source external to the patient, and the radial forces accompanying expansion of the balloons are applied to expand both the graft and the stents radially outward, pressing both elements against the aortic wall 72 proximal to and distal to the aneurysm. The hooks 20 provided on the stent 58 become embedded in the aortic wall 72, to anchor the graft-and-stent combination against downstream arterial pressure while the healing process takes place. In FIG. 11, the delivery apparatus has been withdrawn and the graft-and-stent combination is in final position across the aneurysm and attached to healthy tissue in the aortic wall 72. It should be understood that when the tubular graft 52 is expanded it is not stretching or deforming but is simply opening from

a closed diameter to an open and expanded diameter. The graft material is generally inelastic and can be made from any number of materials compatible with the body such as that manufactured under the trade names D-ACRON® or TEFLON®, and polymeric materials.

[0063] Another preferred method of incorporating a stent embodying the present invention into a graft delivery system is illustrated in FIGS. 12 and 13. This embodiment differs from that shown in FIGS. 8-11 in that a single stent is used to anchor the graft in FIGS. 12-13 while two stents were used in FIGS. 8-11. A single stent is appropriate in the aorta where blood pressures can exceed 100 mm/Hg, which is enough force to hold the proximal end of the graft in place without the need for an anchoring stent on the proximal end of the graft.

[0064] Delivery system 80 (FIGS. 12-13) is shown in the abdominal aorta, just proximal to the aneurysm 54. A single stent 82 is attached by its proximal end 24 to the distal end of the graft 52 by staples, adhesive, or by sewing or other appropriate means as previously described. The graft-and-stent combination is mounted on the catheter 60 and the stent is crimped or compressed onto the balloon 62. A retractable sheath 64 covers and protects both the graft-and-stent combination during delivery through the vascular system until the sheath 64 is withdrawn proximally to allow deployment of the combination. Hooks 20 extend from the most distal cylindrical element 12 to attach the graft and stent to the aortic wall 72. As can be understood with reference to FIGS. 12 and 13, the stent is affixed to the distal end of the graft so that it substantially extends out of the graft, with the result being that radial expansion forces can be applied to the stent by inflating the balloon 62 of the catheter 60 and simultaneously applying expansion force to the graft 52. The stent is expanded simultaneously with the graft to drive the hooks 20 into the aortic wall 72 in healthy tissue distal to the aneurysm 54, to anchor the combination to the vessel.

[0065] Another embodiment using a stent embodying the invention in a graft delivery system is illustrated in FIGS. 14 and 15. The delivery system 90 includes a stent 92 which is coaxial with and which extends the length of and beyond the graft 52, such that the first portion 94 of the stent 92 extends proximally of the graft 52 and the second portion 96 extends distally of the graft. The most distal cylindrical element 12 of the stent 92 is equipped with hooks 20, which will be relied upon at the time of deployment to anchor the graft-and-stent combination to healthy aortic tissue while the prosthesis is accepted by the body of the patient.

[0066] The balloon 98 necessarily must have a much greater length when measured along a longitudinal axis A of the stent 92 than the balloons of previously described embodiments, because the stent of this embodiment is at least double the length of either of the two stents used in the preferred method of delivering the graft and of the stent used in the embodiments of FIGS. 8-13.

[0067] As can be seen with reference to FIG. 15, the stent 92 and the graft 52 which overlies it are positioned so that the graft spans the length of the aneurysm 54. The balloon 98 then is inflated with pressurized fluid or gas to expand both the graft and the stent simultaneously and to force the hooks 20 into engagement with the aortic wall 72 distally of the aneurysm. The expandable member then is deflated and the delivery system withdrawn, leaving the graft-and-stent combination in place in the blood vessel.

[0068] While the invention has been illustrated and described herein in terms of its use as an endoprostheses for implanting a graft to treat an aneurysm, it will be apparent to those skilled in the art that the stent can be used in other instances in other vessels of the body. Because the described stent has attachment elements and the capacity to expand quickly from relatively small diameters to relatively large diameters, the stent is particularly well suited for implantation in almost any vessel where such devices can be used. This feature, coupled with the fact that the stent does not contract or recoil to any great degree after it is radially expanded, provides a highly desirable support member for other types of endoprostheses. Other modifications and improvements may be made without departing from the scope of the invention.

Claims

1. An intravascular stent (10) for implanting in a body lumen, comprising:
 - 30 a plurality of cylindrical elements (12) which are independently expandable in the radial direction and which are interconnected so as to be generally aligned on a common longitudinal axis, each cylindrical element (12) having a serpentine pattern of alternating peaks (16) and valleys (18);
 - 35 a plurality of connecting elements (14) for interconnecting said cylindrical elements (12), said connecting elements (14) configured to interconnect only said cylindrical elements (12) that are adjacent to each other so that said stent (10), when expanded in the radial direction, retains its overall length without appreciable shortening;
 - 40 said stent being characterised in that it further comprises
 - 45 a plurality of hooks (20) for attaching said stent (10) to the body lumen, each hook (20) being provided at a respective peak (16) of a cylindrical element (12) at a first end (22) of said stent (10), said hooks (20) extending from said first end (22) of said stent (10) in a direction away from said stent (10) and generally parallel to said common longitudinal axis.
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2. The stent (10) of claim 1, wherein said plurality of hooks (20) penetrate the body lumen to more securely attach said stent (10) to the body lumen.
3. The stent (10) of claim 2, wherein said hooks (20) are adapted to penetrate through said body lumen.
4. The stent (10) of claim 1, wherein said plurality of hooks (20) each have a plurality of barbs that extend a distance from said hook (20) and adapted to penetrate through the body lumen. 10
5. The stent (10) of claim 1, wherein said plurality of cylindrical elements (12) are capable of retaining their expanded condition over a range of diameters. 15
6. The stent (10) of claim 1, wherein said plurality of connecting elements (14) between adjacent cylindrical elements (12) extend in a direction generally parallel to said common longitudinal axis. 20
7. The stent (10) of claim 1, wherein the stent (10) is formed from a single piece of tubing.
8. The stent (10) of claim 1, wherein said stent (10) is formed from a flat sheet of material. 25
9. The stent (10) of claim 8, wherein said stent (10) is rolled into a cylindrical configuration from said flat sheet of material, said flat sheet of material having a first longitudinal support bar (36) and a second longitudinal support bar (36) which mate when said stent (10) is rolled into said cylindrical configuration. 30
10. The stent (10) of claim 9, wherein said first longitudinal support bar (36) and said second longitudinal support bar (36) are attached by any of welding, soldering, brazing and adhesives.
11. The stent (10) of claim 8, wherein said stent (10) is rolled into a cylindrical configuration from said flat sheet of material, said flat sheet of material having a first longitudinal edge (28) with a plurality of first lap joints (38) and a second longitudinal edge (30) with a plurality of second lap joints (38), said first lap joints (38) and said second lap joints (38) engaging in a mating relationship when said stent (10) is rolled into said cylindrical configuration. 40
12. The stent (10) of claim 1, wherein said stent (10) is formed of a biocompatible material selected from the group of materials consisting of stainless steel, tantalum and thermoplastic polymers. 50
13. The stent (10) of claim 1, wherein said hooks (20) are attached to said first end (22) of said stent (10) by any of welding, brazing, soldering and adhesives. 55
14. The stent (10) of claim 1, wherein said stent (10) is expandable radially outwardly from within by a force so that said stent (10) expands from a first diameter to a second, larger diameter to engage the body lumen.
15. A graft-and-stent assembly for repairing an aortic aneurysm, the assembly comprising:
- an expandable tubular graft (52) having a distal end and a proximal end and having a length sufficient to span the aortic aneurysm so that said distal end and said proximal end may be positioned adjacent healthy aortic tissue; 10
- an expandable stent (58) as claimed in claim 1 affixed to said graft (52), said stent (58) extending for at least a length distally of said graft (52) such that upon expansion of the graft-and-stent combination at least a first portion of said stent (58) will extend distally of said distal end of said graft (52);
- and so that said plurality of hooks (20) on said distally-extending portion of said stent (58) may engage the aortic wall distally of the aneurysm and affix the graft-and-stent combination to repair the aortic aneurysm; and
- catheter means (60) for delivering and deploying said stent (58) and said graft (52), said catheter means (60) having a balloon portion (62) for radially expanding said stent (58) into engagement with the aortic wall. 15
16. The graft-and-stent assembly of claim 15, wherein said plurality of hooks (20) adapted to penetrate the aortic wall thereby affixing the graft-and-stent combination. 20
17. The graft-and-stent assembly of claim 15 or 16, further comprising a proximal stent (56) affixed to said graft (52) at said graft proximal end, said proximal stent (56) extending for at least a length out of said graft (52) such that upon expansion of the graft-and-stent combination, at least a first portion of said proximal stent (56) will extend out of said graft (52), said proximal stent (56) having a plurality of cylindrical elements (12) which are independently expandable in the radial direction and which are interconnected so as to be generally aligned on a common longitudinal axis; and a plurality of connecting elements (14) for interconnecting said cylindrical elements (12), said connecting elements (14) configured to interconnect only said cylindrical elements (12) that are adjacent to each other so that said proximal stent (56), when expanded in the radial direction, retains its overall length without appreciable shortening. 25
18. The graft-and-stent assembly of claim 17, wherein

- said proximal stent (56) has a plurality of hooks (20) on its proximal end for penetrating the aortic wall thereby affixing the graft-and-stent combination to the aortic wall.
19. The graft-and-stent assembly of claim 15 or 16, wherein said expandable stent (58) is disposed coaxially within and affixed to said graft (52).
20. The graft-and-stent assembly of claim 15, wherein said balloon portion (62) assists in forcing said hooks (20) into said aortic wall.
21. The graft-and-stent assembly of any of claims 15 to 20, wherein said catheter means (60) further includes a retractable sheath (64) for retaining said graft-and-stent combination on said catheter means (60), said retractable sheath (64) being adapted to be withdrawn in the proximal direction thereby allowing said stent (58) to radially expand into contact with the aortic wall.
- Patentansprüche**
1. Intravaskulärer Stent (10) zum Implantieren in ein Körperlumen, umfassend:
- eine Vielzahl von zylindrischen Elementen (12), die in radialer Richtung unabhängig expandierbar sind, und die miteinander verbunden sind, so dass sie im Allgemeinen auf einer gemeinsamen Längsachse ausgerichtet sind, wobei jedes zylindrische Element (12) ein Serpentinenmuster mit abwechselnden Gipfeln (16) und Tälern (18) aufweist; eine Vielzahl von Verbindungselementen (14), um die zylindrischen Elemente (12) miteinander zu verbinden, wobei die Verbindungselemente (14) derart angeordnet sind, dass sie nur zylindrische Elemente (12), welche benachbart sind, miteinander verbinden, so dass der Stent (10) seine Gesamtlänge ohne nennenswerte Verkürzung beibehält, wenn er in radialer Richtung expandiert ist; wobei der Stent **dadurch gekennzeichnet ist, dass er darüber hinaus eine Vielzahl von Haken (20) aufweist, um den Stent (10) am Körperlumen zu befestigen, wobei jeder Haken (20) an einem entsprechenden Gipfel (16) eines zylindrischen Elements (12) an einem ersten Ende (22) des Stents (10) vorgesehen ist, wobei die Haken (20) von dem ersten Ende (22) des Stents (10) in einer von dem Stent (10) wegführenden Richtung und im Allgemeinen parallel zu der gemeinsamen Längsachse verlaufen.**
2. Stent (10) nach Anspruch 1, wobei die Vielzahl von Haken (20) in das Körperlumen eindringen, um den Stent (10) sicherer an dem Körperlumen zu befestigen.
3. Stent (10) nach Anspruch 2, wobei die Haken (20) dafür angepasst sind, das Körperlumen zu durchdringen.
4. Stent (10) nach Anspruch 1, wobei die Vielzahl von Haken (20) jeweils eine Vielzahl von Widerhaken aufweisen, die sich um eine Entfernung von dem Haken (20) erstrecken und dafür angepasst sind, das Körperlumen zu durchdringen.
5. Stent (10) nach Anspruch 1, wobei die Vielzahl zylindrischer Elemente (12) in der Lage sind, ihren expandierten Zustand über eine Reihe von Durchmessern beizubehalten.
6. Stent (10) nach Anspruch 1, wobei die Vielzahl von verbindenden Elementen (14) zwischen benachbarten zylindrischen Elementen (12) in einer Richtung verlaufen, die im Allgemeinen parallel zu der gemeinsamen Längsachse ist.
7. Stent (10) nach Anspruch 1, wobei der Stent (10) aus einem einzigen Röhrenstück gebildet ist.
8. Stent (10) nach Anspruch 1, wobei der Stent (10) aus einem flachen Materialblatt gebildet ist.
9. Stent (10) nach Anspruch 8, wobei der Stent (10) von dem flachen Materialblatt aus in eine zylindrische Anordnung gerollt ist, wobei das flache Materialblatt einen ersten Haltestab in Längsrichtung (36) und einen zweiten Haltestab in Längsrichtung (36) aufweist, die eingreifen, wenn der Stent (10) in die zylindrische Anordnung gerollt ist.
10. Stent (10) nach Anspruch 9, wobei der erste Haltestab in Längsrichtung (36) und der zweite Haltestab in Längsrichtung (36) jeweils durch Schweißen, Löten, Hartlöten oder Haftmittel befestigt sind.
11. Stent (10) nach Anspruch 8, wobei der Stent (10) von dem flachen Materialblatt aus in eine zylindrische Anordnung gerollt ist, wobei das flache Materialblatt eine erste Längskante (28) mit einer Vielzahl von ersten Überlappungsverbindungen (38) und eine zweite Längskante (30) mit einer Vielzahl von zweiten Überlappungsverbindungen (38) aufweist, wobei die ersten Überlappungsverbindungen (38) und die zweiten Überlappungsverbindungen (38) in einer Passverbindung eingreifen, wenn der Stent (10) in die zylindrische Anordnung gerollt ist.
12. Stent (10) nach Anspruch 1, wobei der Stent (10)

- aus einem biokompatiblen Material gebildet ist, das aus der Gruppe von Materialien, umfassend Edelstahl, Tantal und thermoplastische Polymere, gewählt ist.
13. Stent (10) nach Anspruch 1, wobei die Haken (20) an dem ersten Ende (22) des Stents (10) jeweils durch Schweißen, Löten, Hartlöten oder Haftmittel befestigt sind.
14. Stent (10) nach Anspruch 1, wobei der Stent (10) radial von innen nach außen durch eine Kraft expandierbar ist, so dass der Stent (10) von einem ersten Durchmesser zu einem zweiten, größeren Durchmesser expandiert, um das Körperlumen einzugreifen.
15. Stent-Graft Anordnung zum Reparieren eines Aortenaneurysmas, wobei die Anordnung umfasst:
- einen expandierbaren, röhrenförmigen Graft (52) mit einem distalen Ende und einem proximalen Ende und einer ausreichenden Länge, um sich über das Aortenaneurysma zu spannen, so dass das distale Ende und das proximale Ende an das Aortengewebe angrenzend positioniert werden können;
- einen expandierbaren Stent (58) nach Anspruch 1, der an dem Graft (52) befestigt ist, wobei sich der Stent (58) wenigstens um eine Länge distal des Grafts (52) erstreckt, so dass sich bei der Expandierung der Stent-Graft Kombination wenigstens ein erster Teil des Stents (58) distal des distalen Endes des Grafts (52) erstreckt; und so dass die Vielzahl von Haken (20) an dem sich distal erstreckenden Teil des Stents (58) die Aortenwand distal des Aneurysmas eingreifen und die Stent-Graft Kombination befestigen können, um das Aortenaneurysma zu reparieren; und
- Kathetermittel (60) zum Einbringen und Anbringen des Stents (58) und des Grafts (52), wobei die Kathetermittel (60) einen Ballonanteil (62) für die radiale Expandierung des Stents (58) zum Eingreifen in die Aortenwand umfassen.
16. Stent-Graft Anordnung nach Anspruch 15, wobei die Vielzahl von Haken (20) dafür angepasst sind, in die Aortenwand einzudringen, wodurch sie die Stent-Graft Kombination daran befestigen.
17. Stent-Graft Anordnung nach Anspruch 15 oder 16, die darüber hinaus einen proximalen Stent (56) umfasst, der an dem Graft (52) am proximalen Graftende befestigt ist, wobei sich der proximale Stent (56) über wenigstens eine Länge aus dem Graft (52) hinaus erstreckt, so dass sich bei Expansion der Stent-Graft Kombination wenigstens ein
- 5 erster Anteil des proximalen Stents (56) aus dem Graft (52) heraus erstreckt, wobei der proximale Stent (56) eine Vielzahl von zylindrischen Elementen (12) aufweist, die unabhängig voneinander in der radialen Richtung expandierbar sind, und die derart miteinander verbunden sind, dass sie im Allgemeinen auf einer gemeinsamen Längsachse angeordnet sind; und eine Vielzahl von Verbindungs-elementen (12), wobei die Verbindungselemente (14) derart ausgebildet sind, dass sie nur die zylindrischen Elemente (12), welche benachbart sind, miteinander verbinden, so dass der proximale Stent (56), seine Gesamtlänge ohne nennenswerte Verkürzung beibehält, wenn er in radialer Richtung expandiert ist.
- 10 18. Stent-Graft Anordnung nach Anspruch 17, wobei der proximale Stent (56) eine Vielzahl von Haken (20) an seinem proximalen Ende aufweist, um in die Aortenwand einzudringen, wodurch die Stent-Graft Kombination an der Aortenwand befestigt ist.
- 15 19. Stent-Graft Anordnung nach Anspruch 15 oder 16, wobei der expandierbare Stent (58) koaxial innerhalb des Grafts (52) angeordnet ist und an diesem befestigt ist.
- 20 20. Stent-Graft Anordnung nach Anspruch 15, wobei der Ballonanteil (62) dabei hilft, die Haken (20) in die Aortenwand zu zwingen.
- 25 21. Stent-Graft Anordnung nach einem der Ansprüche 15 bis 20, wobei das Kathetermittel (60) darüber hinaus eine zurückziehbare Hülle (64) umfasst, um die Stent-Graft Kombination an dem Kathetermittel (60) zu halten, wobei die zurückziehbare Hülle (64) dafür angepasst ist, in proximaler Richtung zurückgezogen zu werden, wodurch ermöglicht wird, dass der Stent (58) radial bis zur Berührung mit der Aortenwand expandiert.
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- Revendications**
- 45 1. Endoprothèse intravasculaire (10) destinée à être implantée dans un lumen de corps, comprenant :
- une pluralité d'éléments cylindriques (12) qui sont extensibles de manière indépendante dans la direction radiale et qui sont interconnectés de façon à être généralement alignés sur un axe longitudinal commun, chaque élément cylindrique (12) possédant une configuration en serpentin de crêtes (16) et de sillons (18) alternés ;
- une pluralité d'éléments de connexion (14) destinés à interconnecter lesdits éléments cylindriques (12), lesdits éléments de connexion (14)
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- étant configurés pour interconnecter uniquement lesdits éléments cylindriques (12) qui sont adjacents les uns aux autres de façon à ce que ladite endoprothèse (10), lorsqu'elle est dilatée dans la direction radiale, conserve sa longueur totale sans rétrécissement appréciable ; ladite endoprothèse étant caractérisée en ce qu'elle comprend en outre une pluralité de crochets (20) destinés à attacher ladite endoprothèse (10) au lumen de corps, chaque crochet (20) étant prévu au niveau d'une crête respective (16) d'un élément cylindrique (12) au niveau d'une première extrémité (22) de ladite endoprothèse (10), lesdits crochets (20) s'étendant depuis ladite première extrémité (22) de ladite endoprothèse (10) dans une direction hors de ladite endoprothèse (10) et généralement parallèle audit axe longitudinal commun.
2. Endoprothèse (10) selon la revendication 1, dans laquelle ladite pluralité de crochets (20) pénètre le lumen de corps pour fixer de manière plus sûre ladite endoprothèse (10) au lumen de corps.
3. Endoprothèse (10) selon la revendication 2, dans laquelle lesdits crochets (20) sont adaptés pour pénétrer à travers ledit lumen de corps.
4. Endoprothèse (10) selon la revendication 1, dans laquelle ladite pluralité de crochets (20) possèdent chacun une pluralité d'ardillons qui s'étendent sur une distance depuis ledit crochet (20) et sont adaptés pour pénétrer à travers le lumen de corps.
5. Endoprothèse (10) selon la revendication 1, dans laquelle ladite pluralité d'éléments cylindriques (12) sont capables de conserver leur état dilaté sur une gamme de diamètres.
6. Endoprothèse (10) selon la revendication 1, dans laquelle ladite pluralité d'éléments de connexion (14) entre les éléments cylindriques adjacents (12) s'étendent dans une direction généralement parallèle audit axe longitudinal commun.
7. Endoprothèse (10) selon la revendication 1, dans laquelle l'endoprothèse (10) est formée à partir d'une pièce unique de tuyau.
8. Endoprothèse (10) selon la revendication 1, dans laquelle ladite endoprothèse (10) est formée à partir d'une feuille plate de matériau.
9. Endoprothèse (10) selon la revendication 8, dans laquelle ladite endoprothèse (10) est enroulée dans une configuration cylindrique à partir de ladite feuille plate de matériau, ladite feuille plate de ma-
- 5 tériau possédant une première barre de support longitudinale (36) et une deuxième barre de support longitudinale (36) qui s'accouplent quand ladite endoprothèse (10) est enroulée dans ladite configuration cylindrique.
10. Endoprothèse (10) selon la revendication 9, dont laquelle ladite première barre de support longitudinale (36) et ladite deuxième barre de support longitudinale (36) sont fixées par un quelconque des moyens de soudage, brasage tendre, brasage et adhésif.
15. Endoprothèse (10) selon la revendication 8, dont laquelle ladite endoprothèse (10) est enroulée dans une configuration cylindrique depuis ladite feuille plate de matériau, ladite feuille plate de matériau possédant une première arête longitudinale (28) avec une pluralité de premiers joints à recouvrement (38) et une deuxième arête longitudinale (30) avec une pluralité de deuxièmes joints à recouvrement (38), lesdits premiers joints à recouvrement (38) et lesdits deuxièmes joints à recouvrement (38) se mettant en prise dans une relation d'accouplement quand ladite endoprothèse (10) est enroulée dans ladite configuration cylindrique.
20. Endoprothèse (10) selon la revendication 1, dont laquelle ladite endoprothèse (10) est composée à partir d'un matériau biocompatible sélectionné depuis le groupe de matériaux comprenant de l'acier inoxydable, du tantalum et des polymères thermoplastiques.
25. Endoprothèse (10) selon la revendication 1, dont laquelle lesdits crochets (20) sont attachés à ladite première extrémité (22) de ladite endoprothèse (10) par l'un quelconque des moyens de soudage, brasage tendre, brasage et adhésif.
30. Endoprothèse (10) selon la revendication 1, dans laquelle ladite endoprothèse (10) est extensible de manière radiale vers l'extérieur depuis l'intérieur par une force afin que ladite endoprothèse (10) se dilate depuis un premier diamètre vers un deuxième diamètre plus grand pour mettre en prise le lumen de corps.
35. Ensemble de greffon et endoprothèse destiné à réparer un anévrisme d'aorte, l'ensemble comprenant :
40. un greffon tubulaire extensible (52) possédant une extrémité distale et une extrémité proximale et présentant une longueur suffisante pour écarter l'anévrisme de l'aorte de façon à ce que ladite extrémité distale et ladite extrémité proximale puissent être positionnées de manière ad-

- jacente au tissu sain de l'aorte ; une endoprothèse extensible (58) selon la revendication 1, fixée audit greffon (52), ladite endoprothèse (58) s'étendant sur au moins une longueur distale dudit greffon (52) de manière à ce qu'à la dilatation de la combinaison greffon et endoprothèse au moins une première partie de ladite endoprothèse (58) s'étende de manière distale par rapport à ladite extrémité distale dudit greffon (52) ; et de sorte que ladite pluralité de crochets (20) sur ladite partie s'étendant de manière distale de ladite endoprothèse (58) puisse mettre en prise la paroi aortique distale de l'anévrisme et fixer l'ensemble greffon et endoprothèse pour réparer l'anévrisme aortique ; des moyens formant cathéter (60) destinés à délivrer et déployer ladite endoprothèse (58) et ledit greffon (52), lesdits moyens formant cathéter (60) possédant une partie formant ballon (62) pour dilater de manière radiale ladite endoprothèse (58) lors de la mise en prise avec la paroi de l'aorte.
16. Ensemble greffon et endoprothèse selon la revendication 15, dans lequel ladite pluralité de crochets (20) sont adaptés pour pénétrer la paroi de l'aorte fixant ainsi la combinaison greffon et endoprothèse.
17. Ensemble greffon et endoprothèse selon la revendication 15 ou 16, comprenant en outre une endoprothèse proximale (56) fixée audit greffon (52) au niveau de ladite extrémité proximale du greffon et, ladite endoprothèse proximale (56) s'étendant sur au moins une longueur dudit greffon (52) de manière à ce qu'à la dilatation de la combinaison greffon et endoprothèse, au moins une première partie de ladite endoprothèse proximale (56) s'étende en dehors dudit greffon (52), ladite endoprothèse proximale (56) possédant une pluralité d'éléments cylindriques (12) qui sont extensibles de manière indépendante dans la direction radiale et qui sont interconnectés de manière à être généralement alignés sur un axe longitudinal commun ; et une pluralité d'éléments de connexion (14) pour interconnecter lesdits éléments cylindriques (12), lesdits éléments de connexion (14) étant configurés pour interconnecter uniquement lesdits éléments cylindriques (12) qui sont adjacents les uns aux autres de façon à ce que ladite endoprothèse proximale (56), lors de la dilatation dans la direction radiale, conserve sa longueur globale sans rétrécissement appréciable.
18. Ensemble greffon et endoprothèse selon la revendication 17, dans lequel ladite endoprothèse proximale (56) possède une pluralité de crochets (20) sur son extrémité proximale destinés à pénétrer la paroi de l'aorte fixant ainsi la combinaison greffon
- et endoprothèse à la paroi de l'aorte.
19. Ensemble greffon et endoprothèse selon la revendication 15 ou 16, dans lequel ladite endoprothèse expansible (58) est placée de manière coaxiale à l'intérieur du et fixée audit greffon (52).
20. Ensemble greffon et endoprothèse selon la revendication 15, dans lequel ladite partie formant ballon (62) aide à forcer lesdits crochets (20) dans ladite paroi d'aorte.
21. Ensemble greffon et endoprothèse selon l'une quelconque des revendications 15 à 20, dans lequel lesdits moyens formant cathéter (60) comprennent en outre une gaine rétractable (64) destinée à retenir ladite combinaison greffon et endoprothèse sur lesdits moyens formant cathéter (60), ladite gaine rétractable (64) étant adaptée pour être retirée dans la direction proximale permettant ainsi à ladite endoprothèse (58) de se dilater de manière radiale au contact de la paroi de l'aorte.

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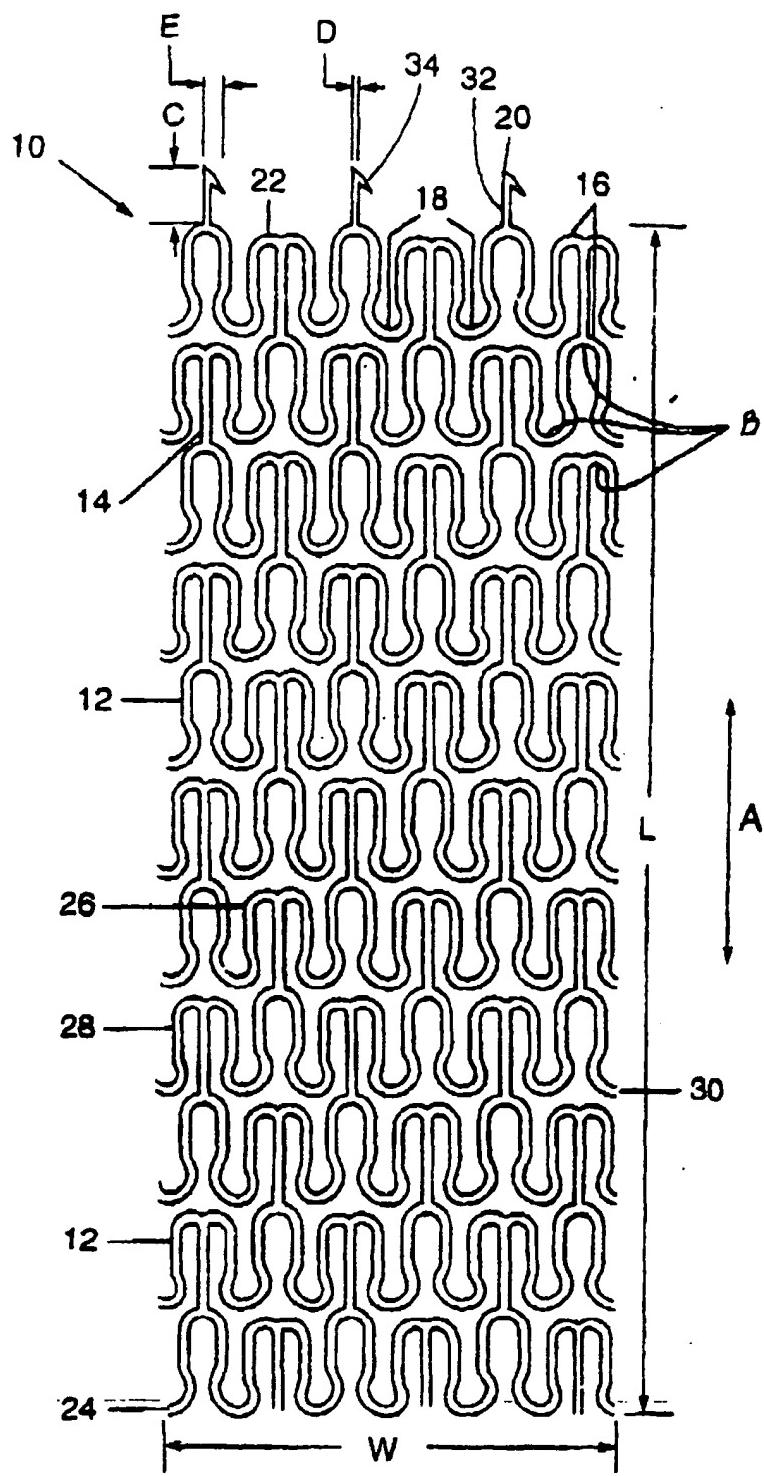


Fig. 1

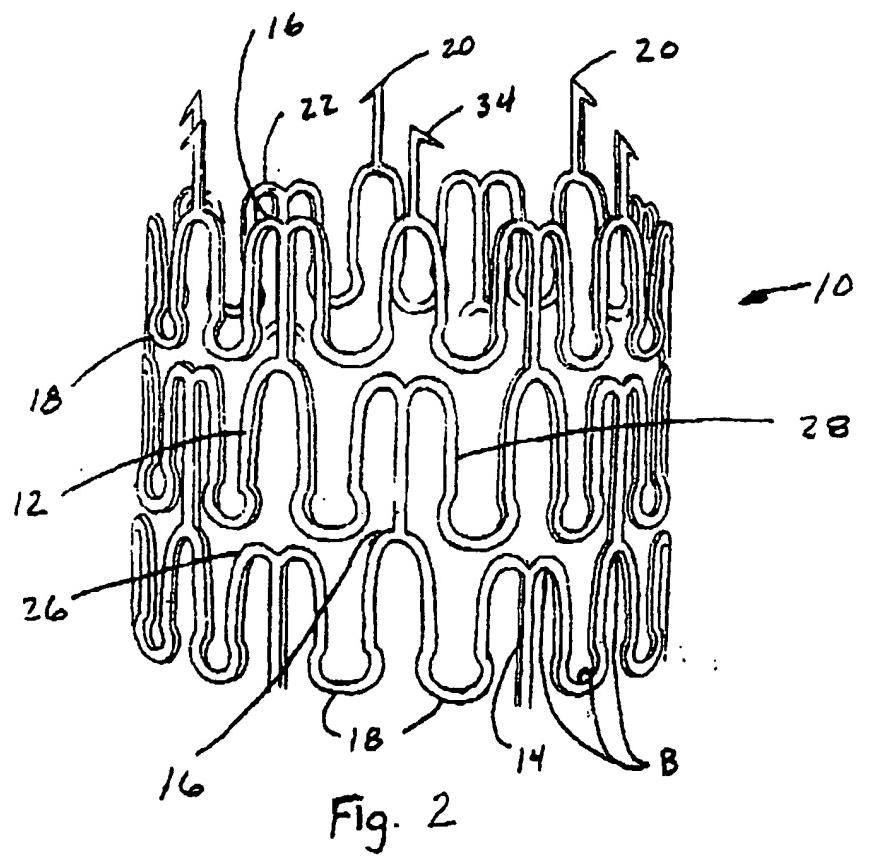


Fig. 2

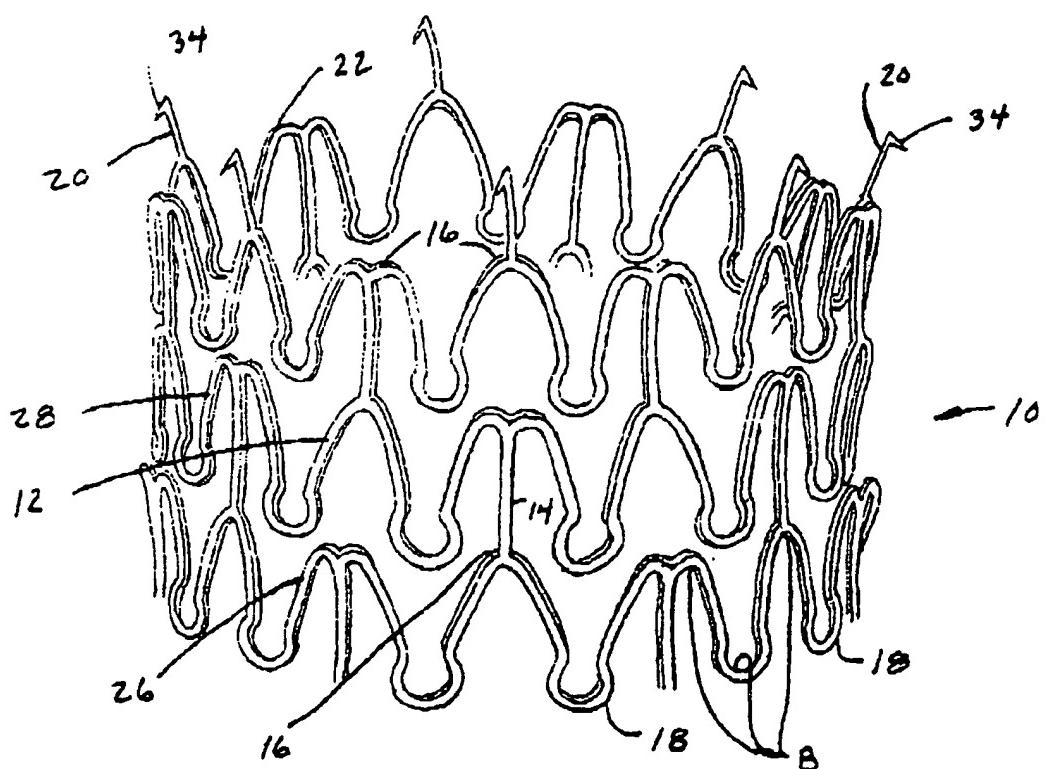


Fig 3

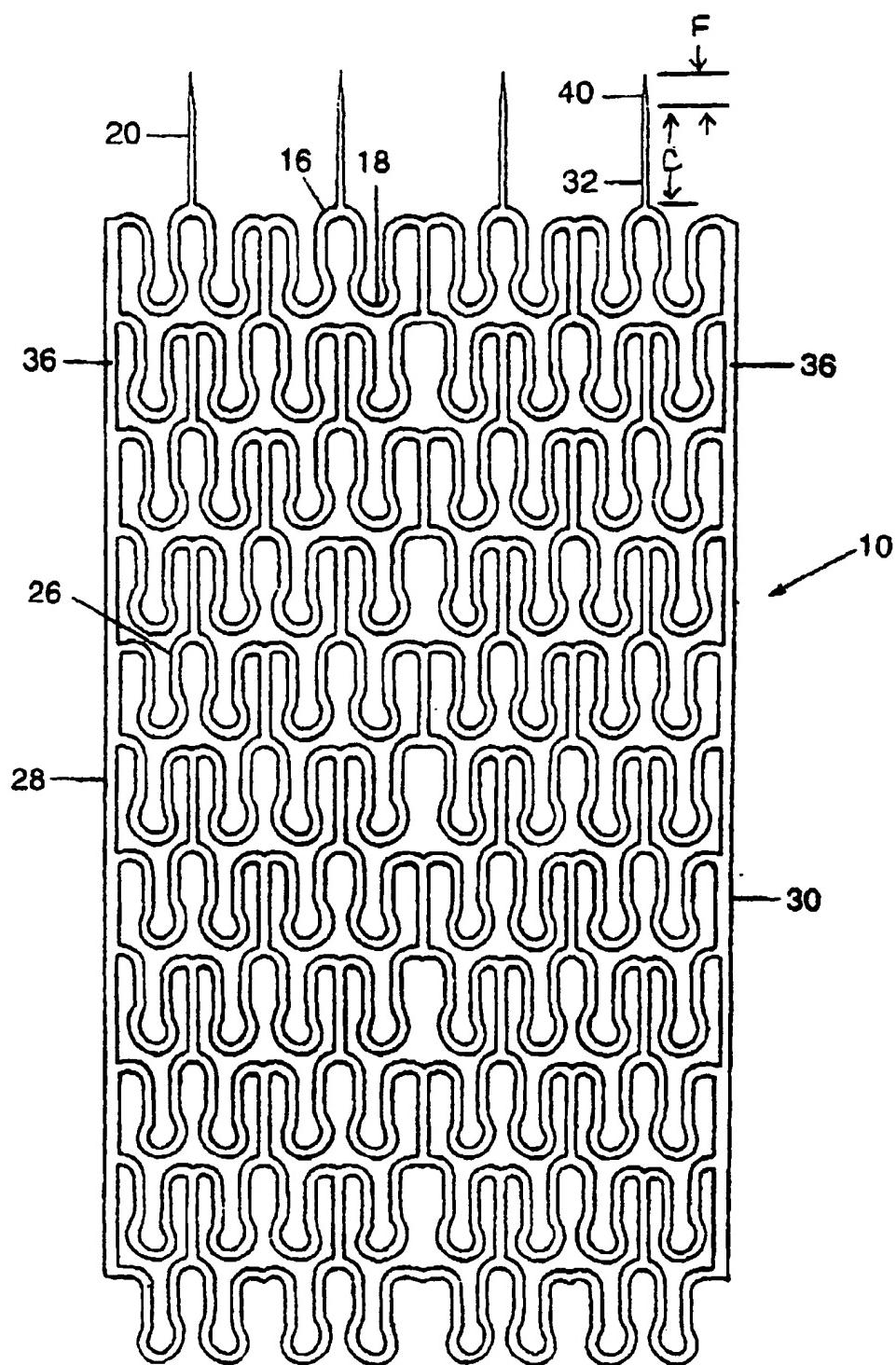


Fig.4

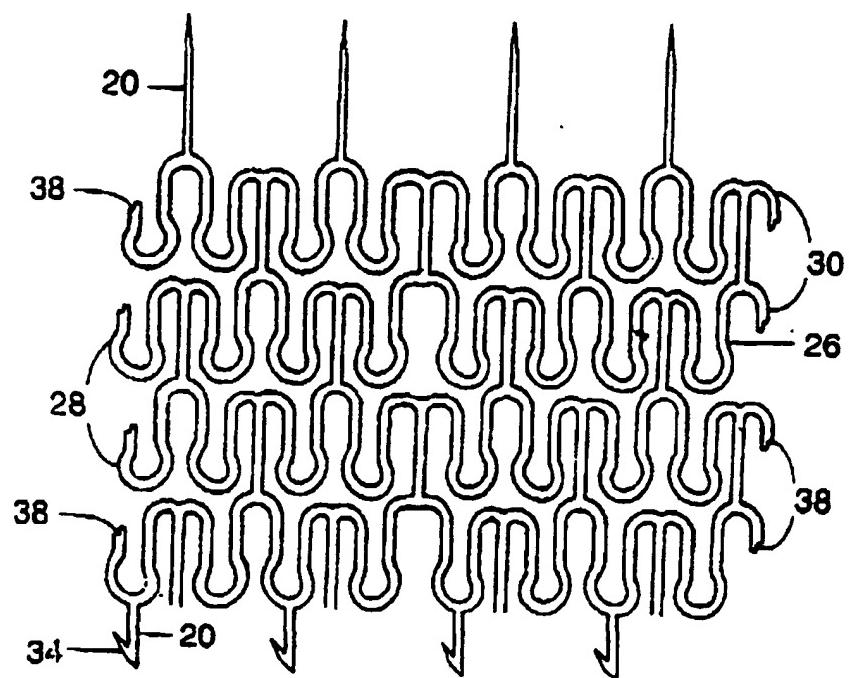


Fig.5

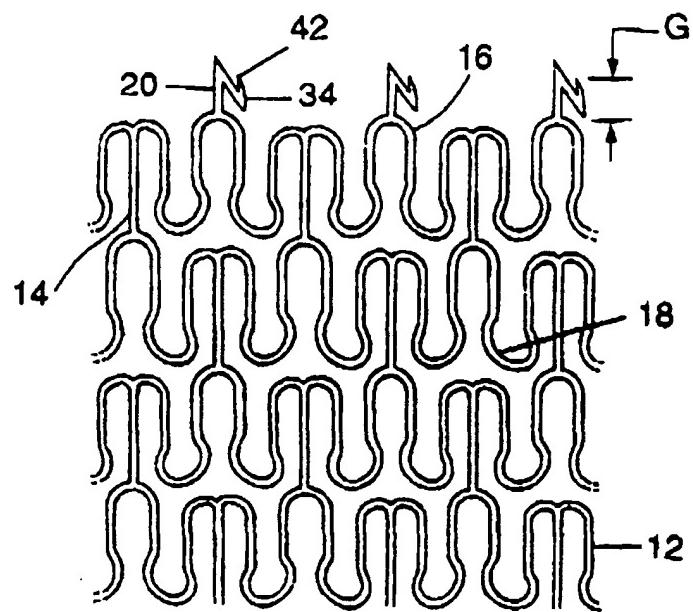


Fig. 6

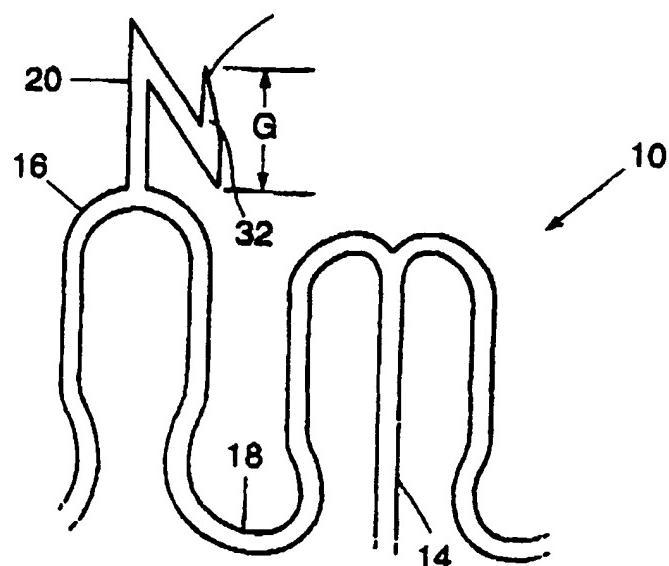
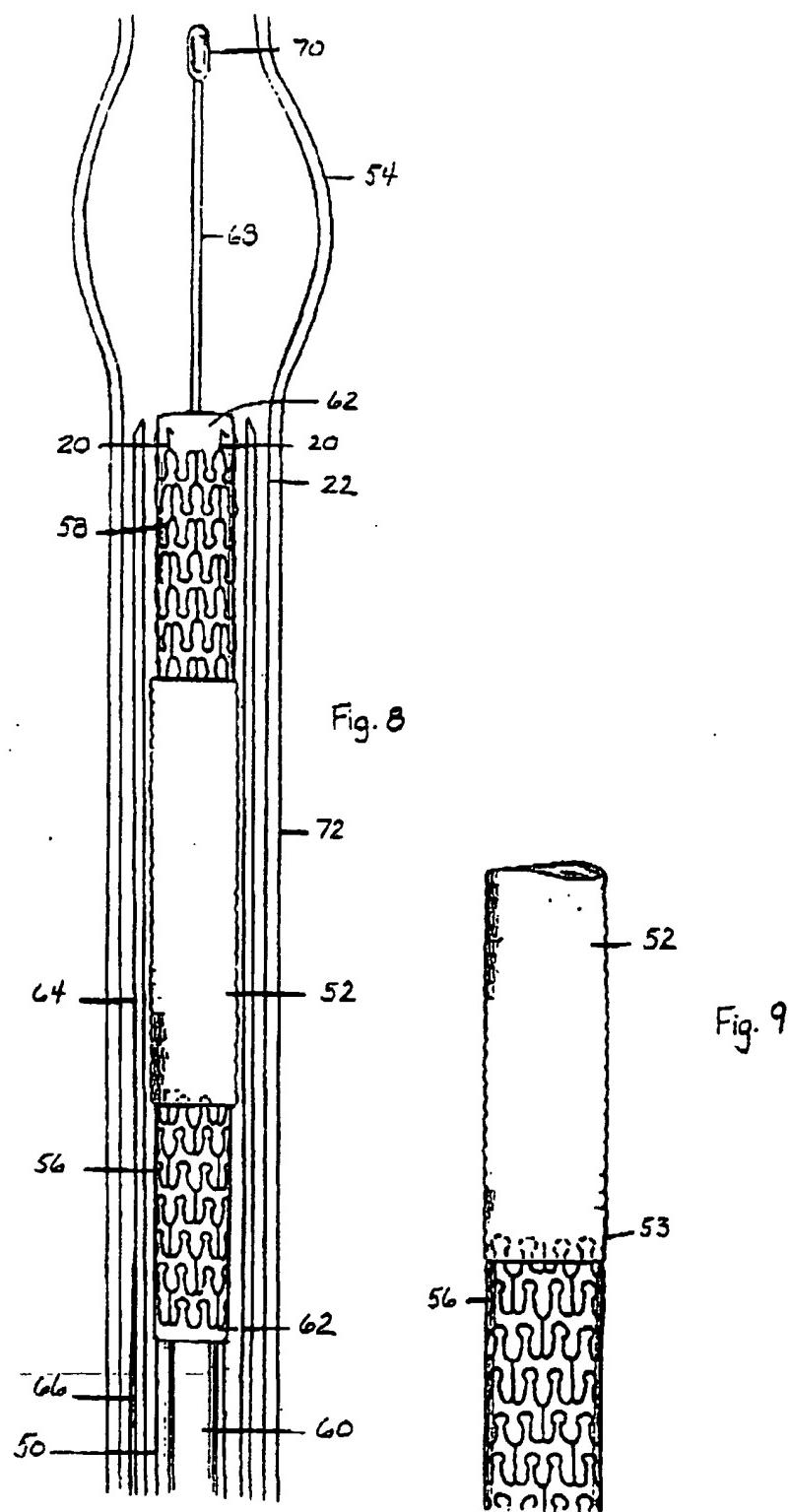


Fig. 7



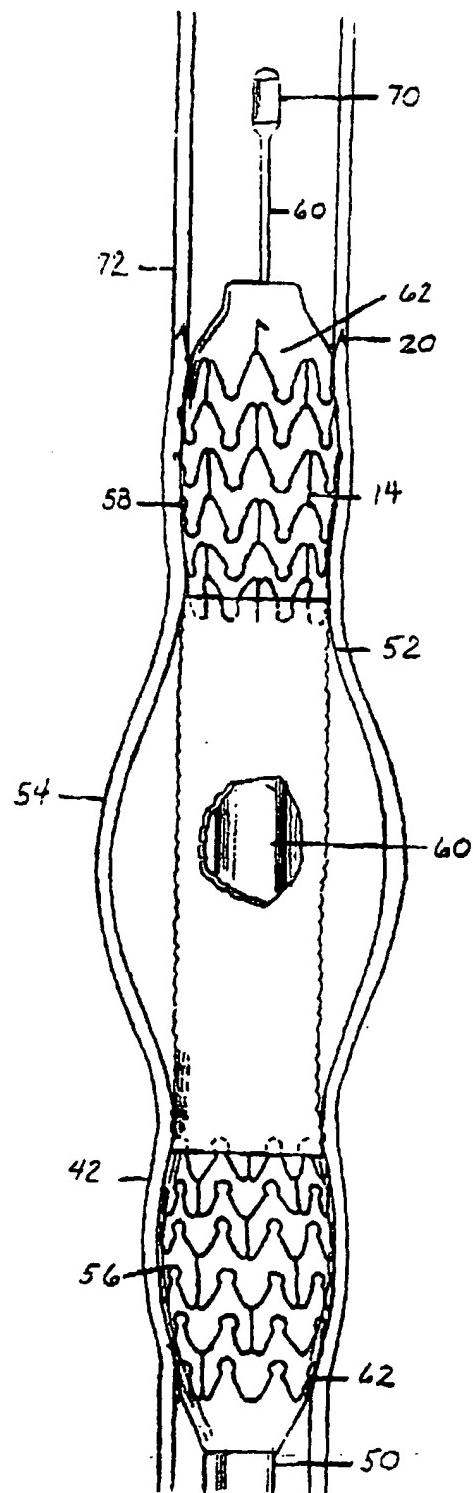
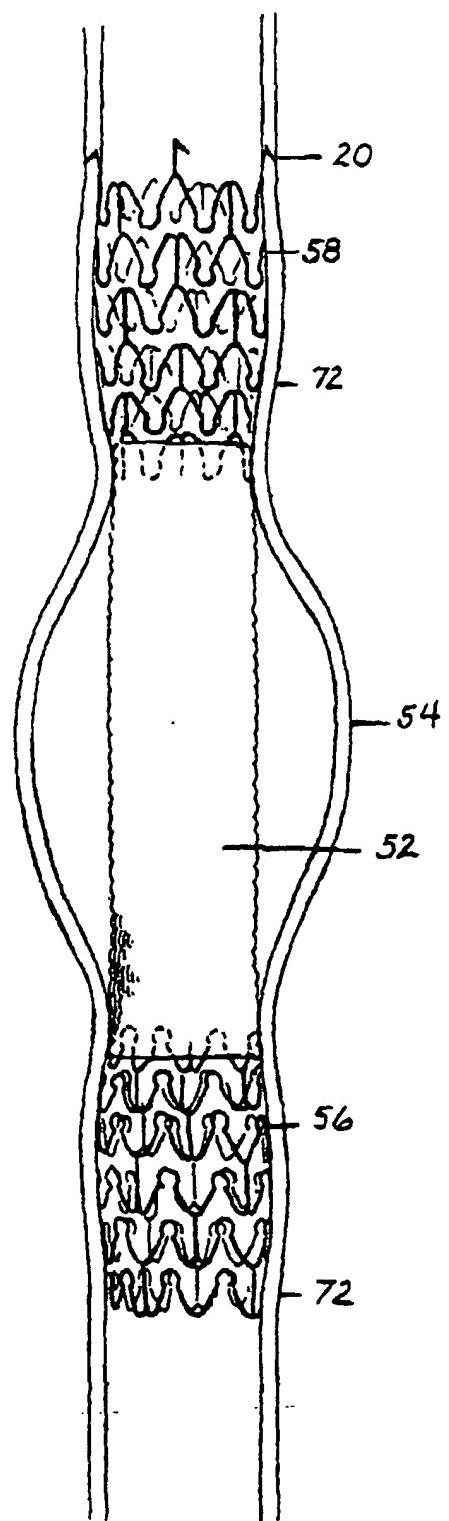


Fig. 10



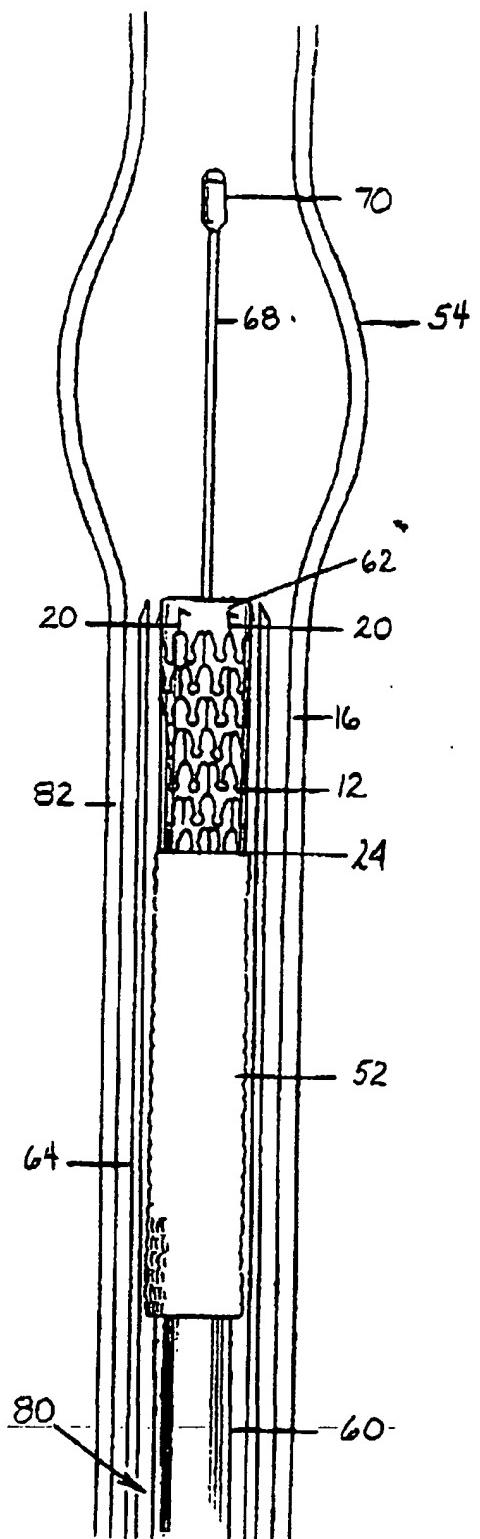


Fig. 12

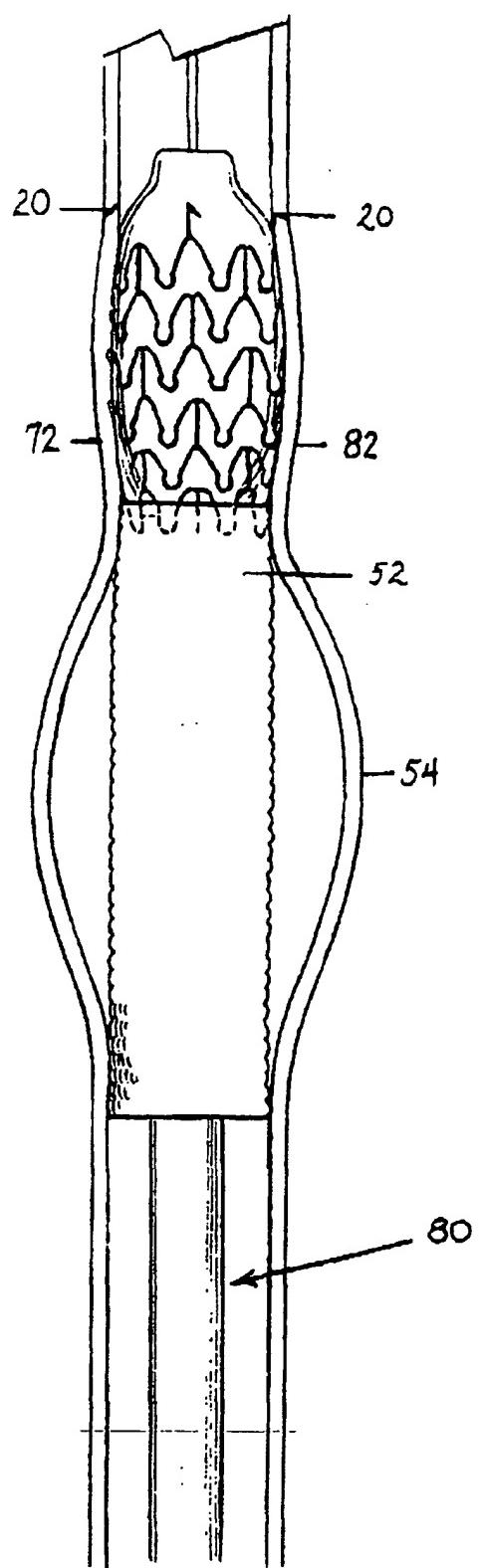


Fig.13

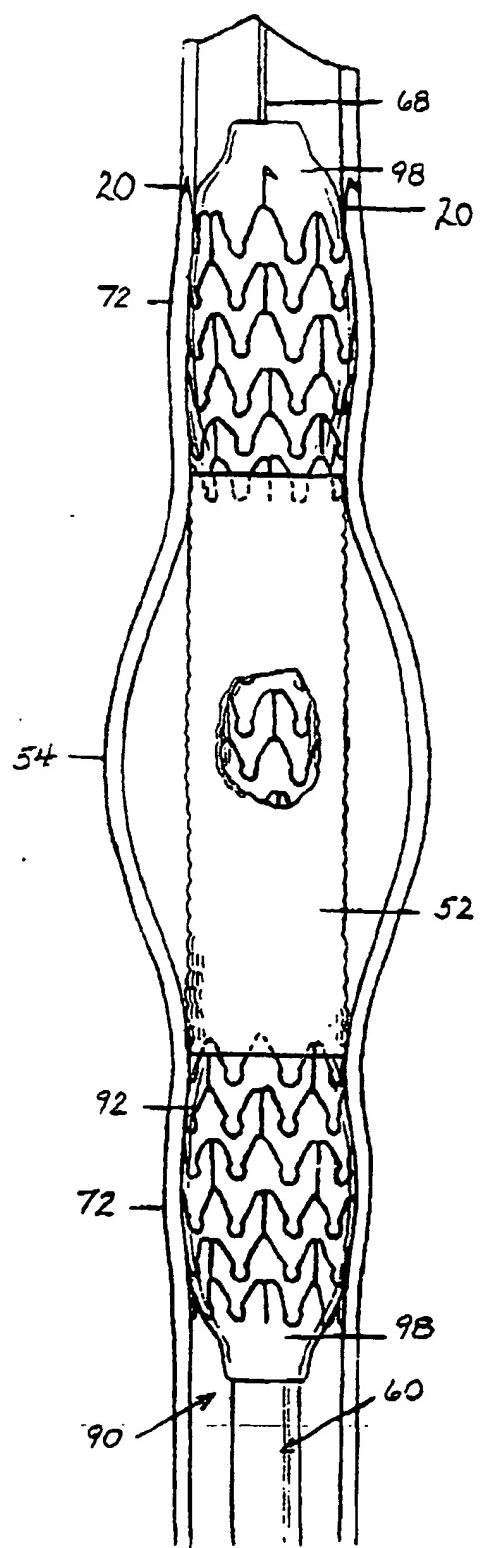


Fig. 15

